

Next-Generation Robotic Surgery

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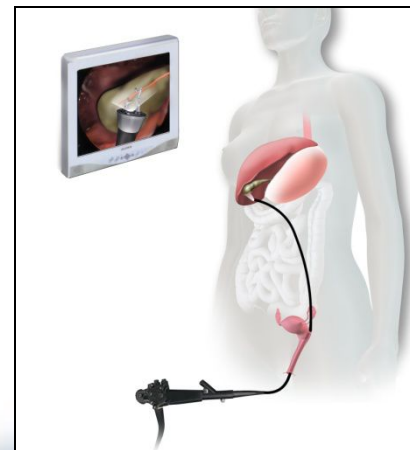
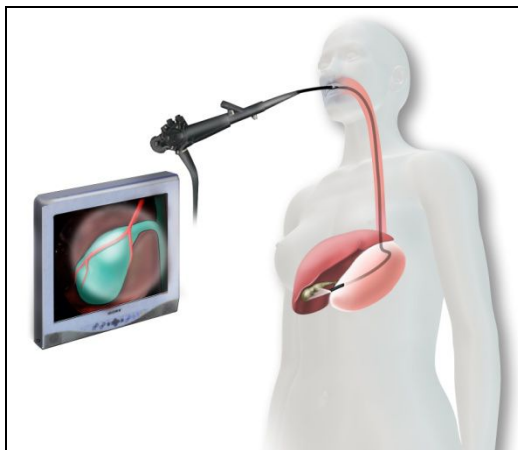


Talk Overview

1. In-vivo imaging device (mono)
2. In-vivo imaging device (stereo)
3. Insertable Robotic Effector Platform (IREP)
4. Markerless Surgical Tool Tracking
5. Continuum Surgical Robot Pose Estimation using Vision

Surgical Robotics: Research Goals

- Create **simple-to-use** and **cost-effective** surgical robots
- Convert more “major access” operations to “minimal access” operations.
- Reduce the invasiveness of current minimal access interventions
 - ◆ **SPA: Single Port Access** for laparoscopic surgery
 - ◆ **NOTES: Natural Orifice Transluminal Endoscopic Surgery**
 - ◆ Use natural body openings with robotic platforms

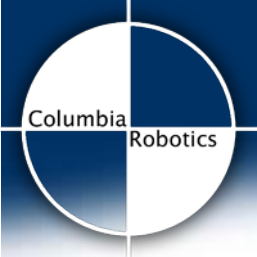


Current Generation Robotic Surgery

Devices such as DaVinci®
Huge leap in robotics, but:

- ◆ Large footprint in the OR
- ◆ Cost is extremely high
- ◆ Requires multiple incisions
- ◆ Multiple assistants needed
- ◆ Uses traditional endoscope with limited mobility within body cavity
- ◆ Has not reduced the invasiveness of robotic MIS
- ◆ While this paradigm has been enormously successful, and has spurred development of new methods and devices, it is **ultimately limiting in what it can achieve**





Next-Generation Robotic Surgery

- Surgery will be radically different in the future
- New thrusts in computer & robotic technologies can make automated surgery, if not feasible, an approachable goal.
- Vision: **teams of insertable robots** performing surgical tasks in the body under both surgeon & computer control.
- Remotize sensors and effectors in the body cavity where they can perform surgical & imaging tasks **unfettered by traditional endoscopic instrument design.**

Building New In-vivo Devices

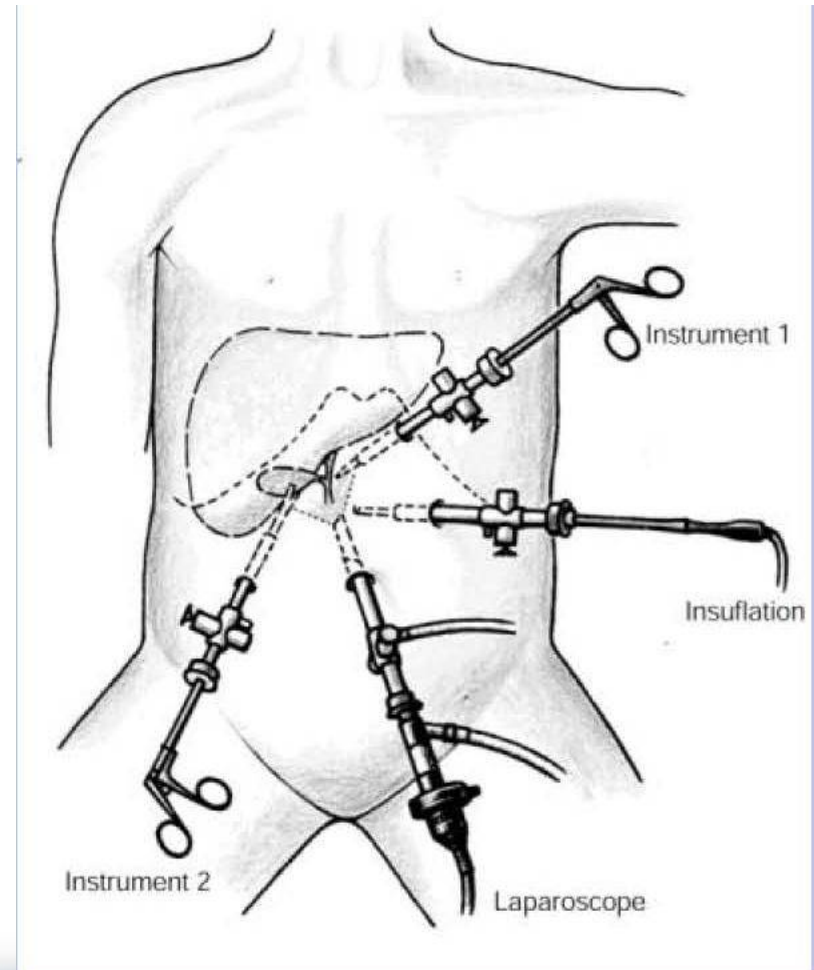
- Current minimal access surgery adheres to the Chopstick Paradigm:
Pushing long sticks into small openings



Problems with Current Imaging Devices

Can we improve on the traditional laparoscope?

- Laparoscope Issues:
 - ◆ Narrow angle imaging
 - ◆ Limited workspace
 - ◆ Multiple incisions for camera placements
 - ◆ Counter intuitive motion for control
 - ◆ Trained assistants needed to control the camera
 - ◆ Multiple incisions for camera placements
 - ◆ Additional incisions needed for laparoscopic instruments.



In-Vivo Imaging Devices



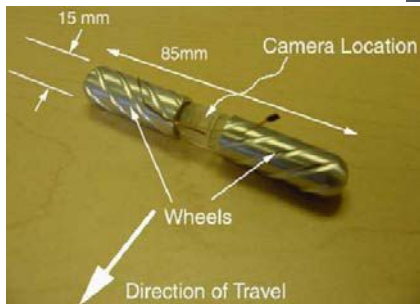
Flexible Endoscope



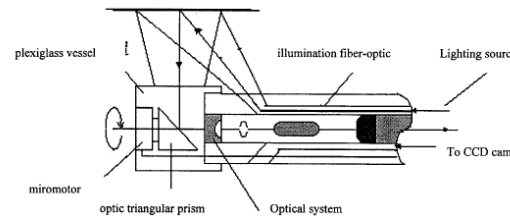
Karl Storz Endoscope



Pill camera

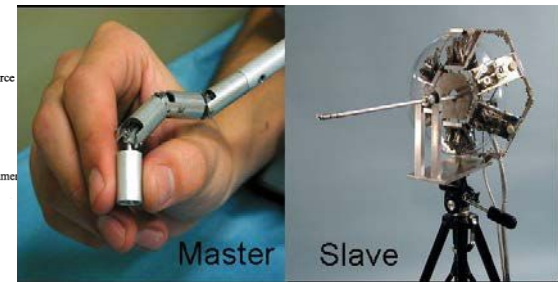


U. Nebraska

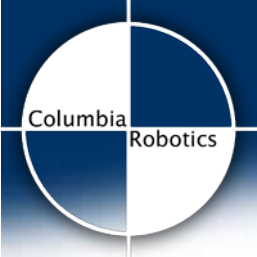


Gao et al., 1998

- Rod-lens by Hopkins and cold light source of fiber optics by Karl Storz.
- Flexible endoscope using fiber optics to delivery light and transmit image.
- Pill camera without locomotion.
- Endoscope with rotating mirror.
- Endoscope positioned by multilink arm with piezoelectric actuators.
- Mobile robots, U. Nebraska



Ikuta et. al., 2002



Columbia Imaging Device: Design Goals

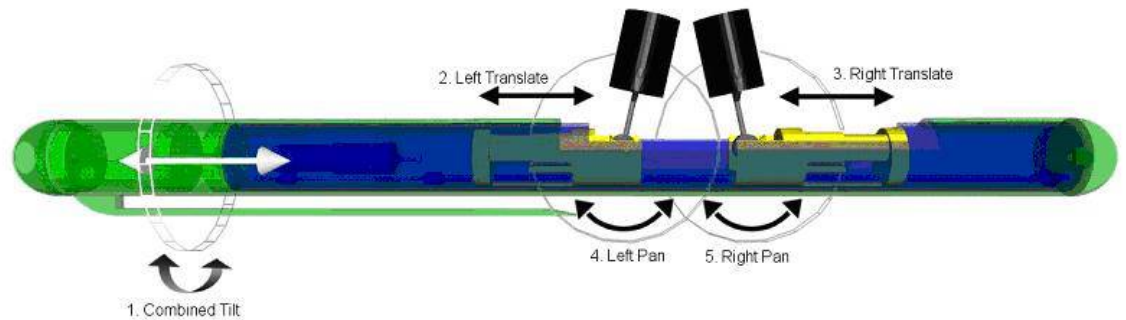
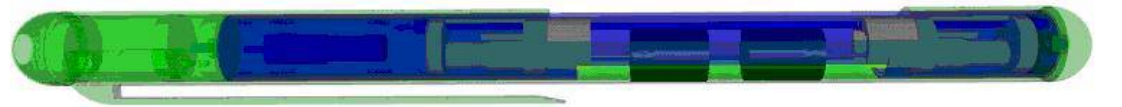
- Device must be fully insertable into body cavity, leaving the insertion port free for other sensors and tooling
- Device diameter must be restricted to 15 mm diameter for use with standard trocars.
- Pan and Tilt degrees of freedom needed to increase internal imaging field of view
- Image Zoom function required
- Integrated lighting
- Simple intuitive control interface to operator
- Real-time computer control of DOF's to allow tracking and visual servoing
- User friendly 2D/3D display system
- Low cost and possible disposal use



Columbia Imaging Device Overview

- Design 0: Paper design, 2 cameras, 5-DOF
- Device 0: Single camera prototype, 3-DOF, tested in surgical trainer
- Device I: Single camera, pan/tilt/lighting, tested in animals
- Device II: Single camera, pan/tilt/zoom, tested in animals
- Device III: Stereo cameras, pan/tilt, tested in animals

Design 0



Design of 5-DOF insertable camera device



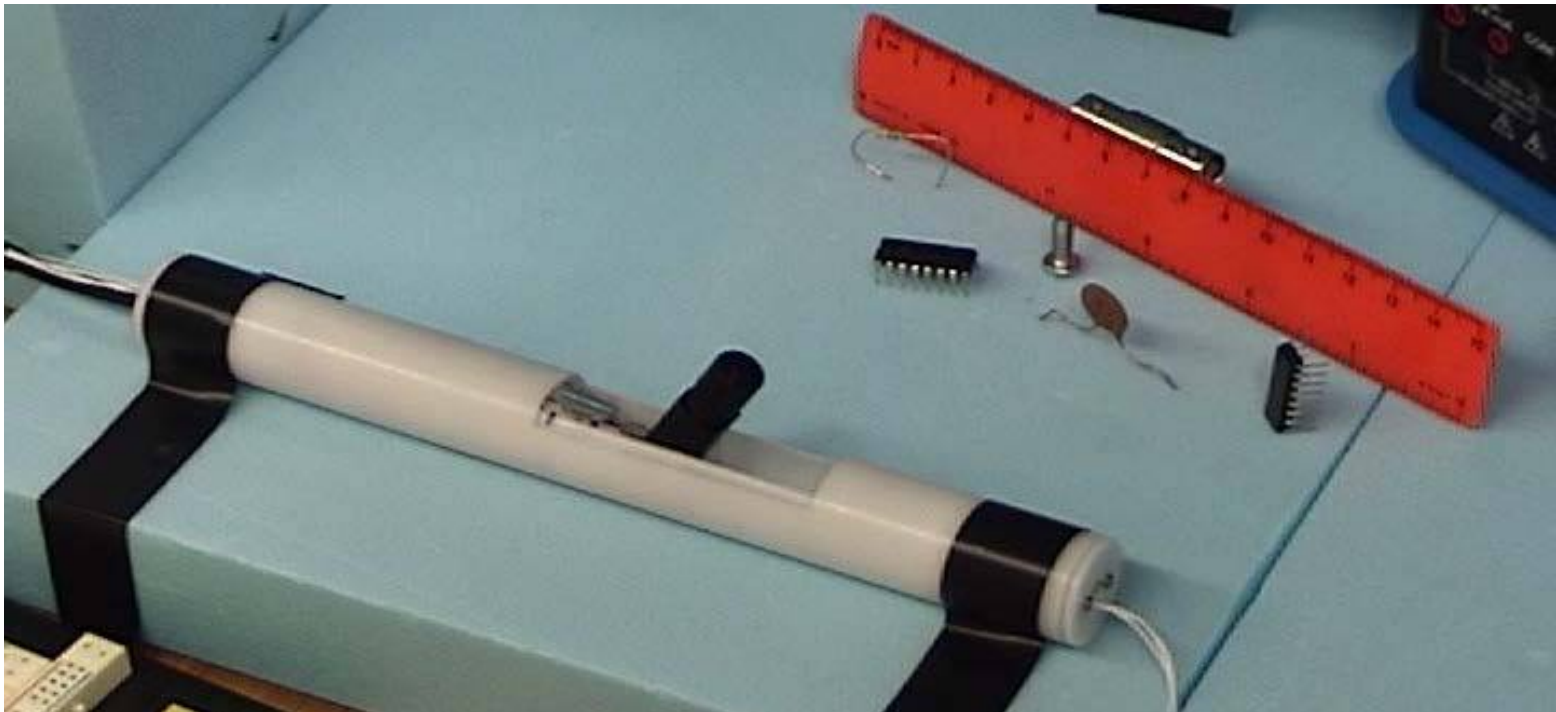
- Stereo cameras with 6 DOF are desirable – full mobility
- Difficult to achieve in small actuated package
- Compromise – 3 DOF per camera
 - ◆ Cameras share tilt axis (1 DOF)
 - ◆ Independent translation (2 DOF)
 - ◆ Independent pan (2 DOF)

Device I: Single Camera

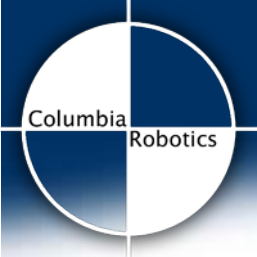
Diameter: 22 mm; Length: 190 mm

Camera opening: 58 mm

3 DOF: Pan: 120°; Tilt: 130°; Translation: 50 mm



[Video](#)



Initial Testing and Validation

Does new imaging device improve surgery visualization?

- ◆ 6 fellows & surgeons performed MISTELS* tests with standard laparoscope and the new robotic camera
- ◆ 5 of 6 subjects showed no significant difference in MISTELS task performance with the robotic camera compared to the standard laparoscope
- ◆ Mean score of 999 +/- 69 using a laparoscope
- ◆ Mean score of 953 +/- 68 for the robotic camera: statistically insignificant difference

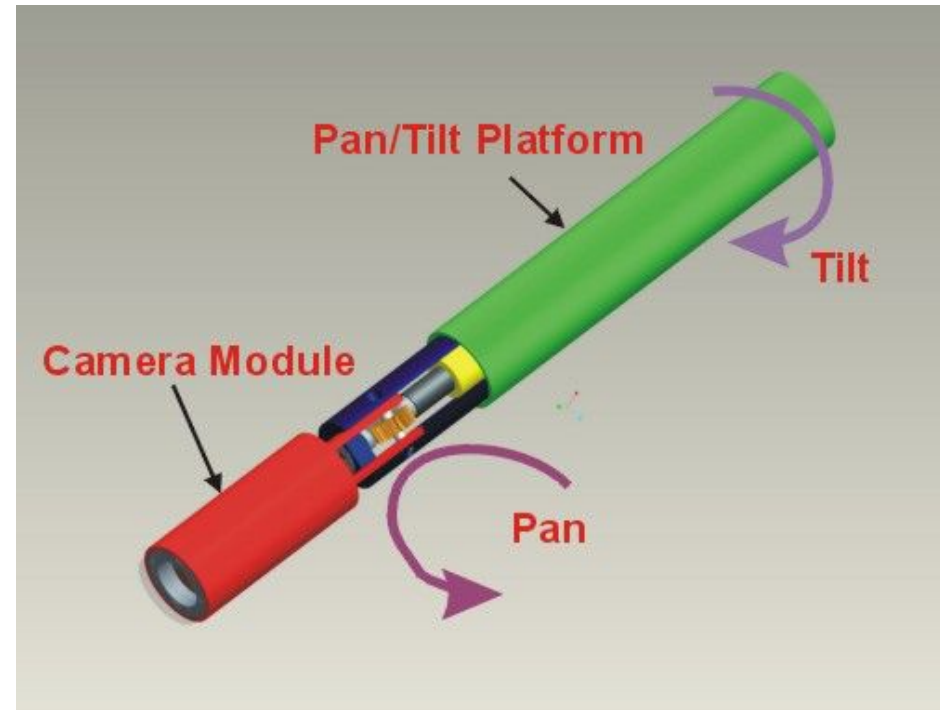
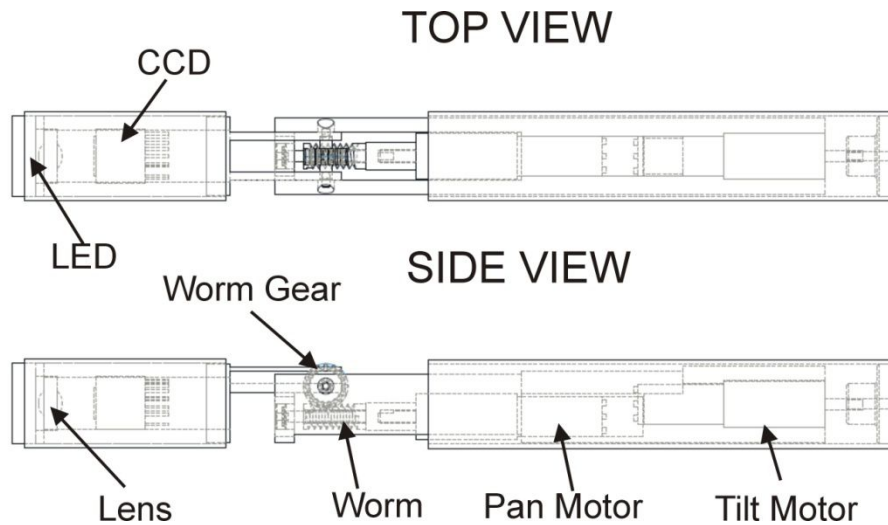
**McGill Inanimate System for the Training and Evaluation of Laparoscopic Skill*



Device I: Design Goals

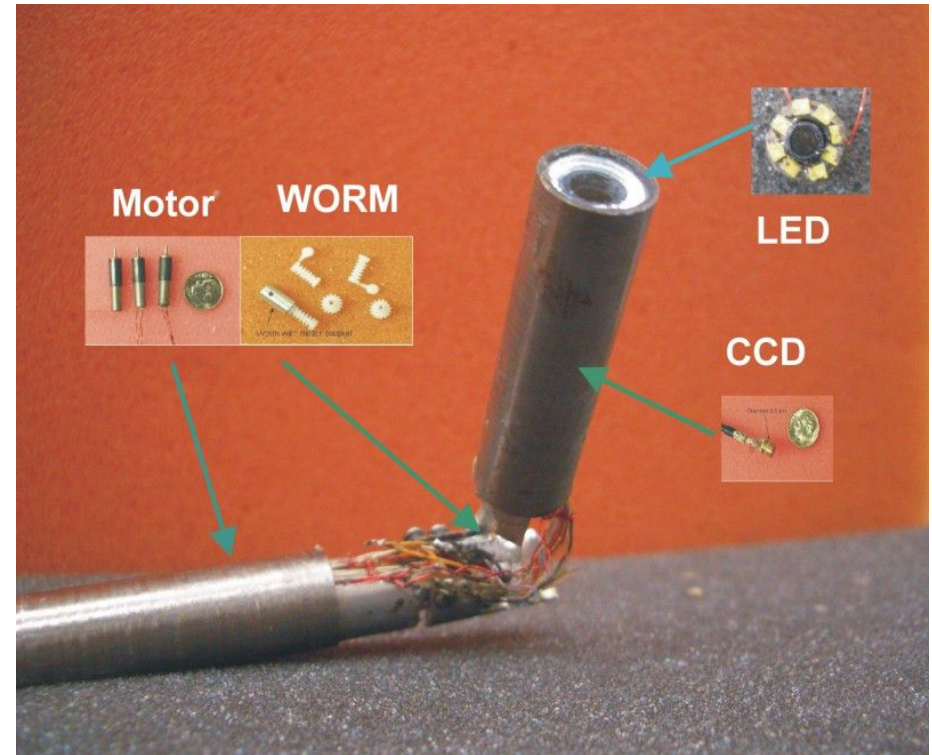
- Need to reduce size to fit 12mm trocar
- Motors are major determinant of device size
- Removing a camera reduced motor count by 2
- Translation DOF is least useful. Removing this also reduced motor count by 1
- Include integrated light source
- Make imaging head modular
- Tradeoff: Degrees-of-freedom for compactness

Device I: Single Camera



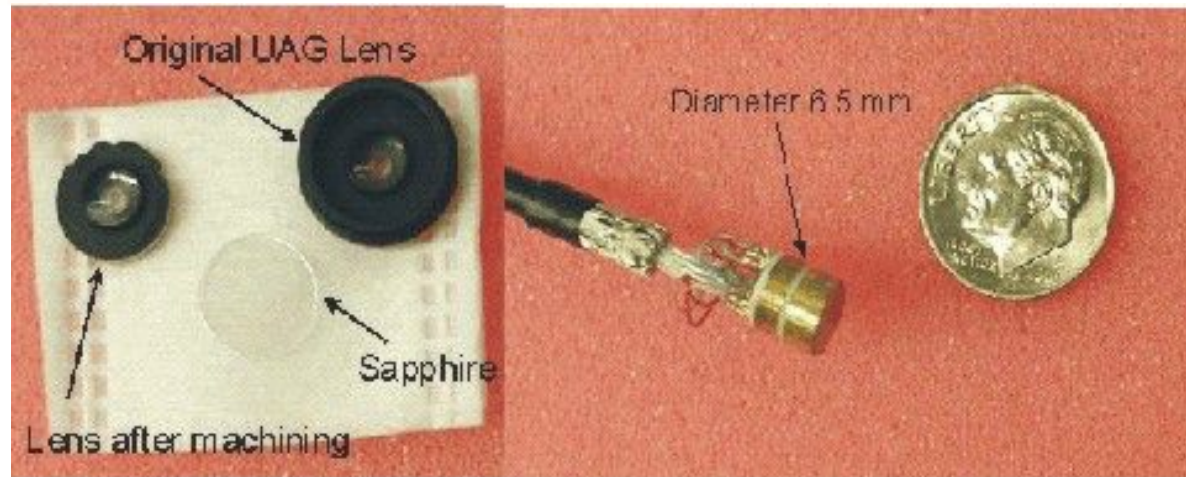
Device I: Single Camera*

- 110 mm in length and 11 mm in diameter.
- 130 degree Pan, 90 degree Tilt.
- Integrated 8 LED light source.
- 6.5 mm CCD sensor.
- Fully sealed camera head.
- Joystick control.



*Tie Hu, Peter K. Allen, Nancy Hogle and Dennis Fowler Surgical Imaging Device with Pan, Tilt, Zoom, and Lighting, Intl. Journal of Robotics Research, 2009

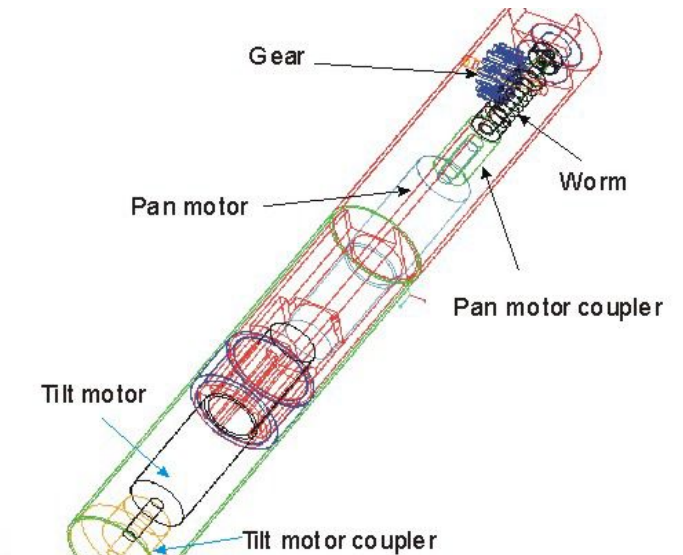
Lens and Camera Unit



- Pin hole lens
 - Focal length 5.0 mm, F number 4.
 - ◆ Angle of view D-H-V(85.4-68.3-50.9).
- 6.5 mm CCD camera sensor.
 - ◆ 450 TV lines in horizontal resolution and 420 TV lines in vertical resolution.
- Fully sealed package to isolate body fluid and moisture.

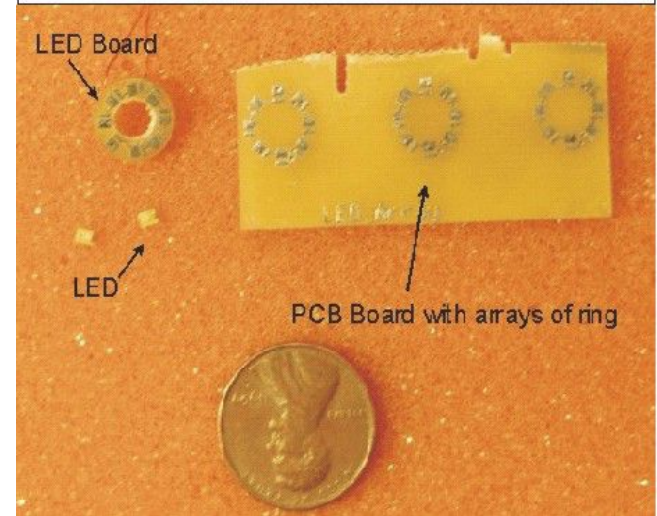
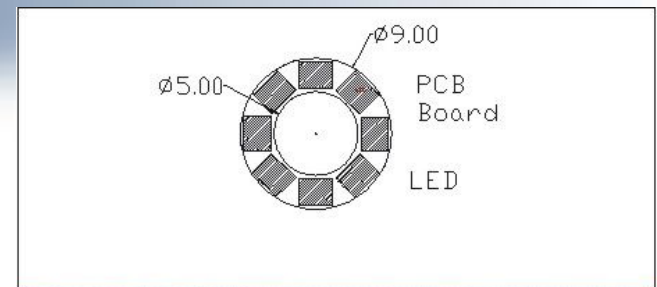
Pan/Tilt Mechanism

- Miniature Brushless DC motor (0513G, Faulhaber Group).
 - ◆ 25mNm torque.
 - ◆ 5.8 mm in diameter.
- Miniature worm gear (Kleiss Gear Inc.)
 - ◆ gear ratio 16:1.

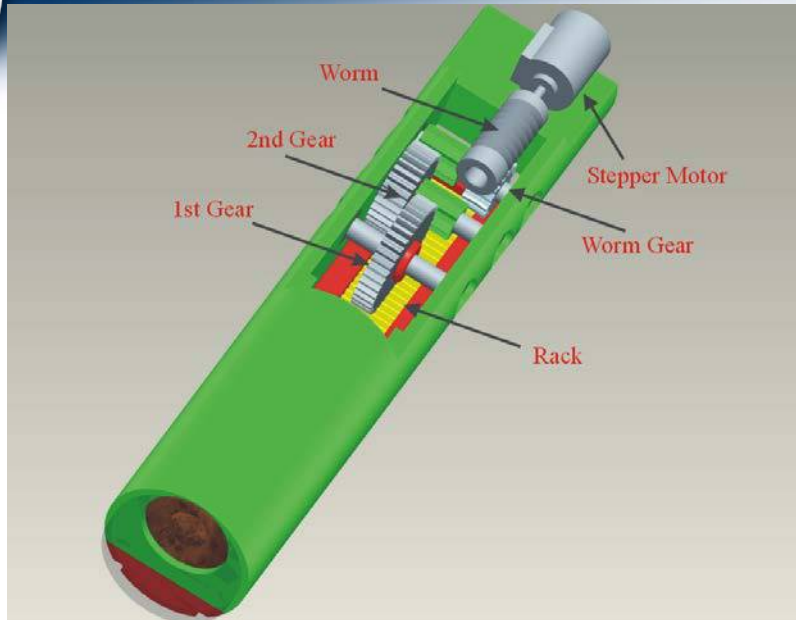


LED Light Source

- Light-emitting diode (LED) as a light source in laparoscopy:
 - ◆ Lower power
 - ◆ Higher efficiency
 - ◆ Compact package
 - ◆ Longer lifespan
 - ◆ Lower cost
- Luxeon portable PWT white LED(LXCL_PWT1)
 - ◆ 2.0 X1.6 X 0.7 mm
 - ◆ 26 lumens of light at 350 mA
- 8 PWT LED in a printed circuit board with 9mm diameter.
 - ◆ 208 lumens light at 8.4 w



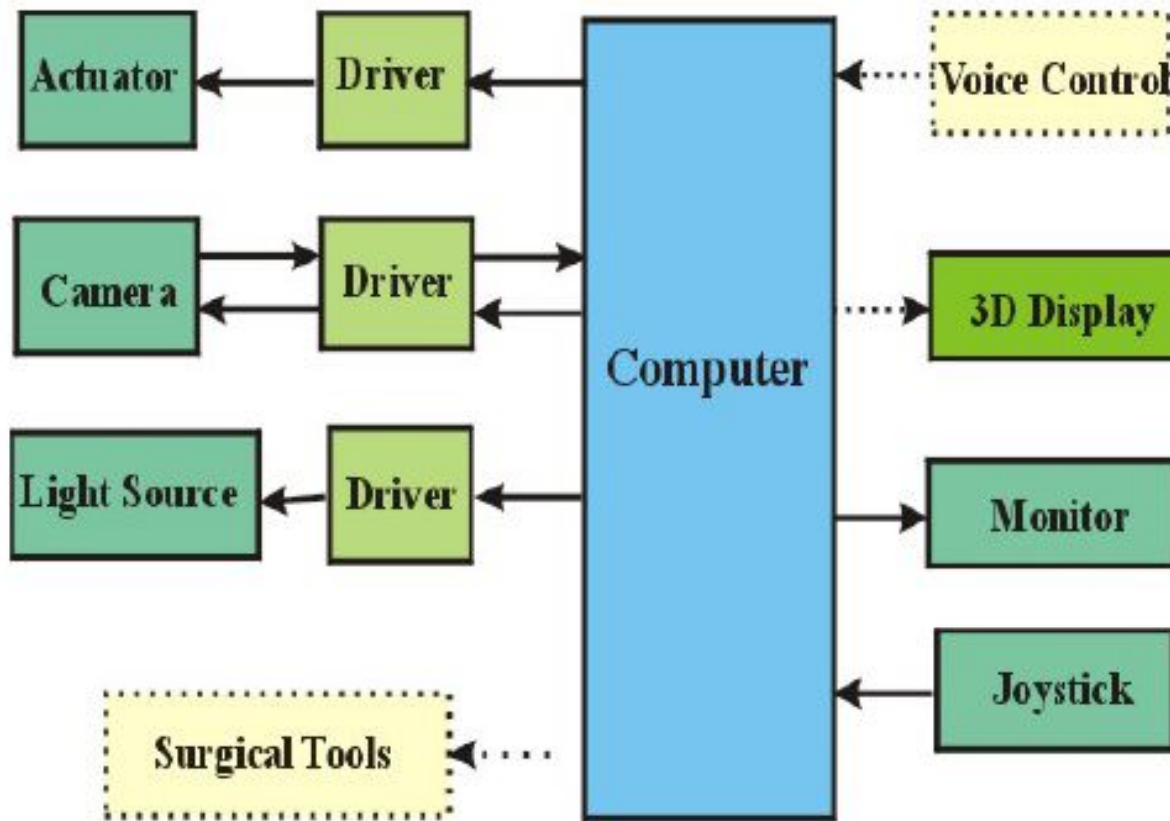
Device II: Pan, Tilt, Zoom



- Mechanical zoom: linear motion of camera head
- Stepper motor drives rack and pinion mechanism
- Can only achieve $\sim 2x$ zoom



System Architecture



No expensive console needed, just a standard PC!



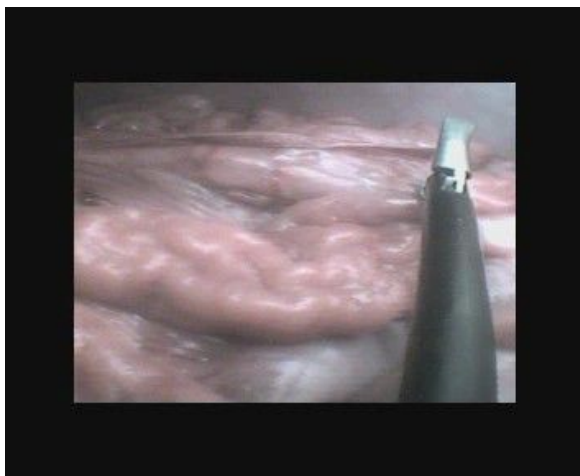
Mounting the Camera

- Camera attached to insufflated abdominal wall
- Attachment methods:
 - ◆ Suturing: small stitch through abdomen
 - ◆ Magnets
 - ◆ “Fish Hook” which grabs the abdominal wall
 - ◆ Intelligent trocar for attachment

Suturing the Camera



In-Vivo Animal Experiments

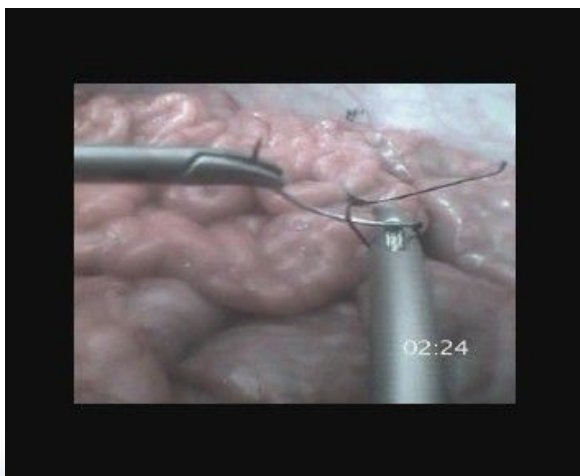


Bowel Running



Appendectomy

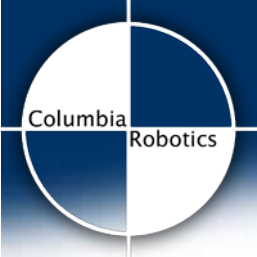
[Video](#)



Suturing



Nephrectomy



Procedure Timings

Procedure	Device	Time (min)
Running Bowel	Laparoscope	4:20
Running Bowel	Robot	3:30
Appendectomy	Laparoscope	2:20
Appendectomy	Robot	2:20
Suturing	Laparoscope	5:00
Suturing	Robot	4:00
Nephrectomy	Laparoscope	18:00
Nephrectomy	Robot	21:00



Intelligent Software

- Position/Velocity control of axes
- Intuitive Joystick Control
- Real-Time Image Processing:
 - ◆ Digital Zoom
 - ◆ Image rotation/stabilization
 - ◆ Distortion Correction
 - ◆ Picture-in-Picture
 - ◆ Visual Servoing/Tracking
 - ◆ 3D Stereo output

Image Processing

Zoom :



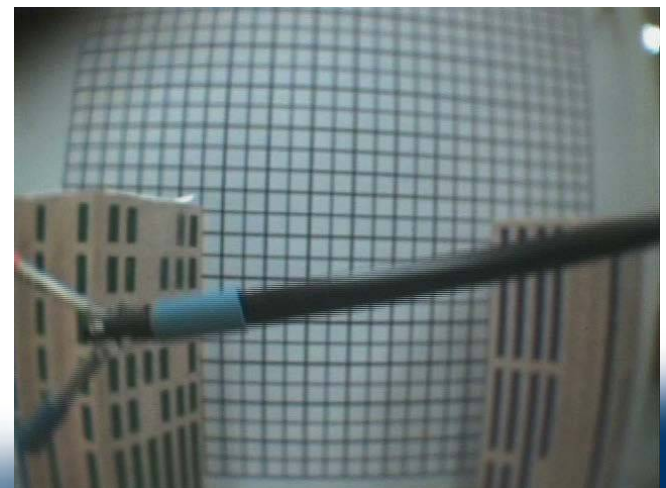
Picture in Picture :

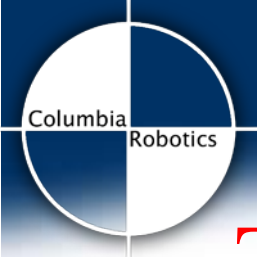


Rotation :



Distortion Correction :





Tracking Instruments using Color Markers

- Place colored marker on instrument
- Convert RGB to HSV space
- Hue value of a pixel is much less susceptible to lighting changes
- Record hue value of marker to be tracked
- Search entire image for hue values within epsilon range
- Centroid of matched pixels gives position of tracker in the image
- If target is detected, localize search to a smaller neighborhood
- Tracking performed in real-time at 25 fps



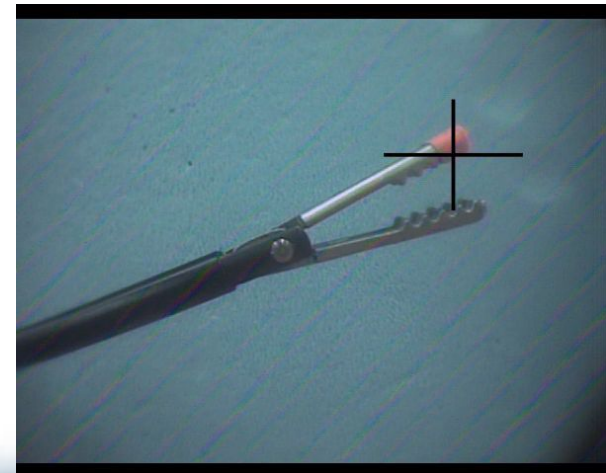
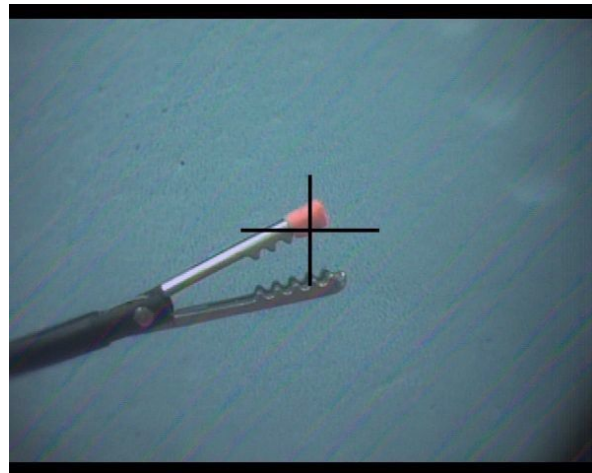
Visual Servoing

- Allows shared autonomy with surgeon
- The feedback from the tracker can be used to drive motors to keep the tool in the center of the image
- PD controller used
- (E_x, E_y) : offset error of tracker from center of image

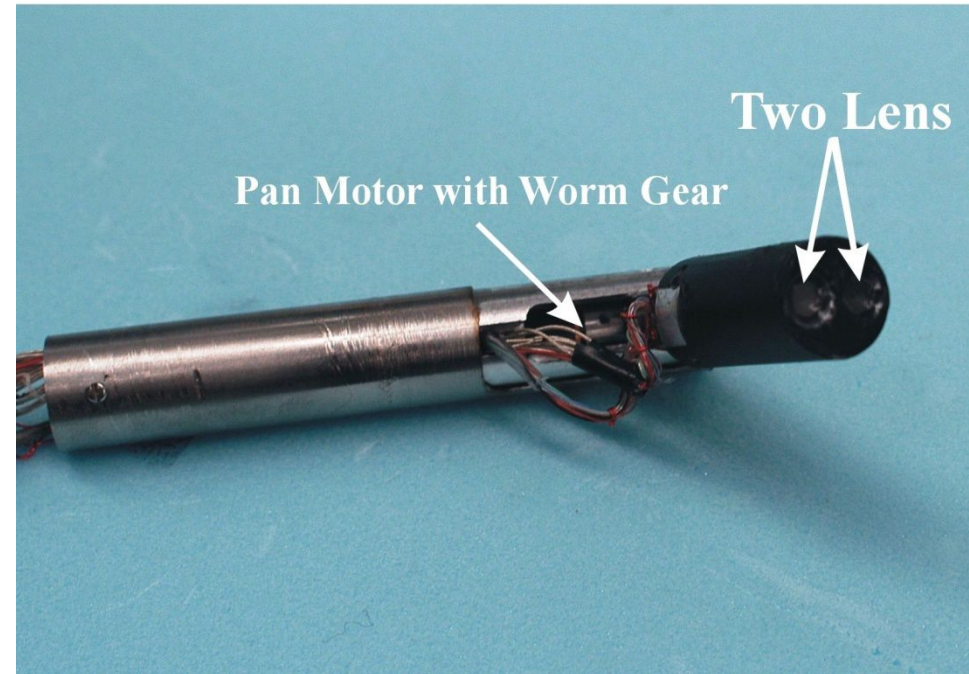
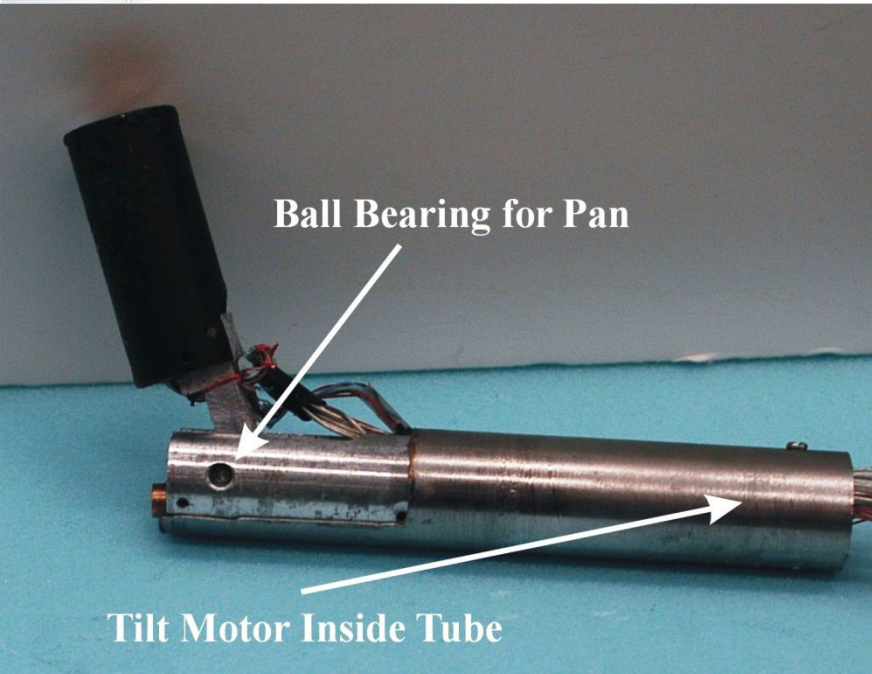
$$\text{Pan speed} \propto (\alpha_x * E_x) - (\beta_x * dE_x/dt)$$

$$\text{Tilt speed} \propto (\alpha_y * E_y) - (\beta_y * dE_y/dt)$$

- Video



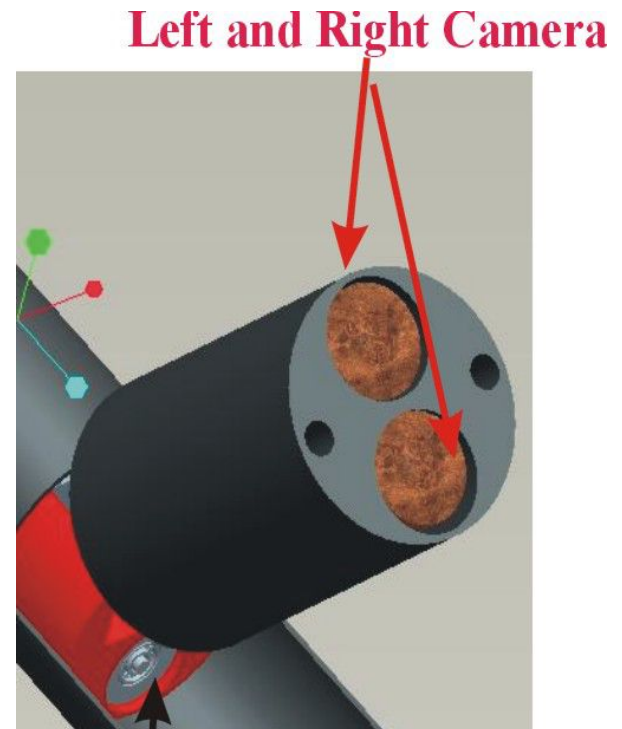
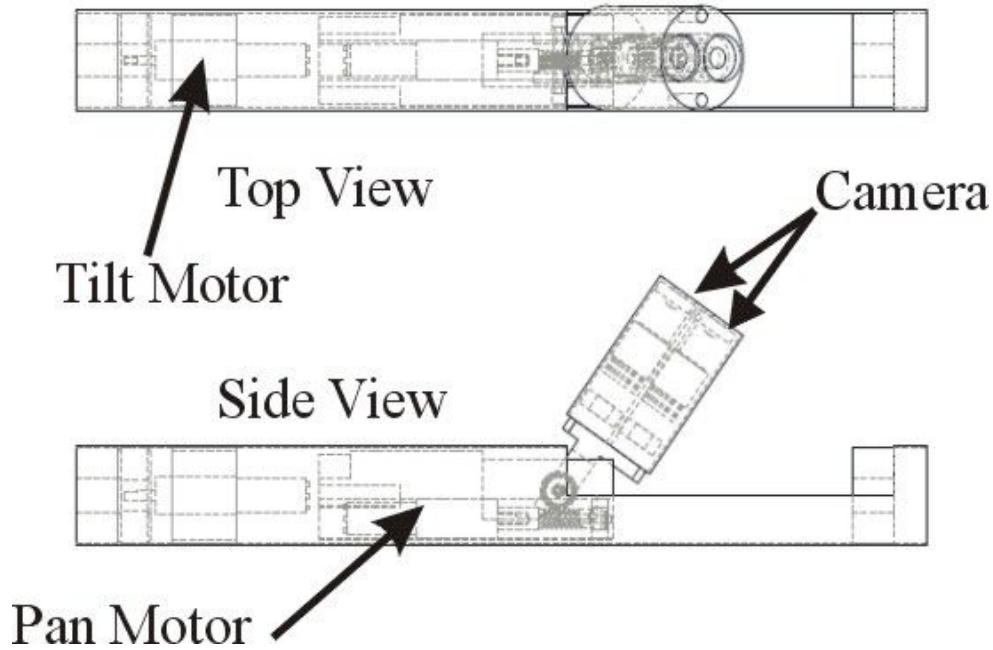
Device III: Stereo Imaging*



- A stereo imaging device with similar mechanical design.
- 15 mm in diameter and 120 mm in length.
- 6.5mm Inter-Pupillary Distance (IPD)

*T. Hu, P. Allen,, T. Nadkarni, N. Hogle, D. Fowler, *Insertable Stereoscopic 3D Surgical Imaging Device*, IEEE BIOROB 2008

Stereo Camera

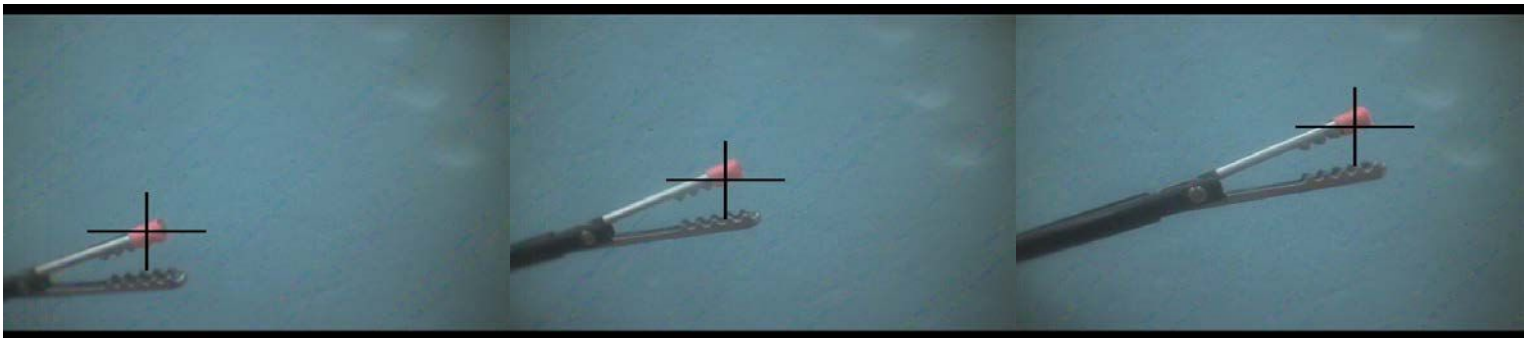
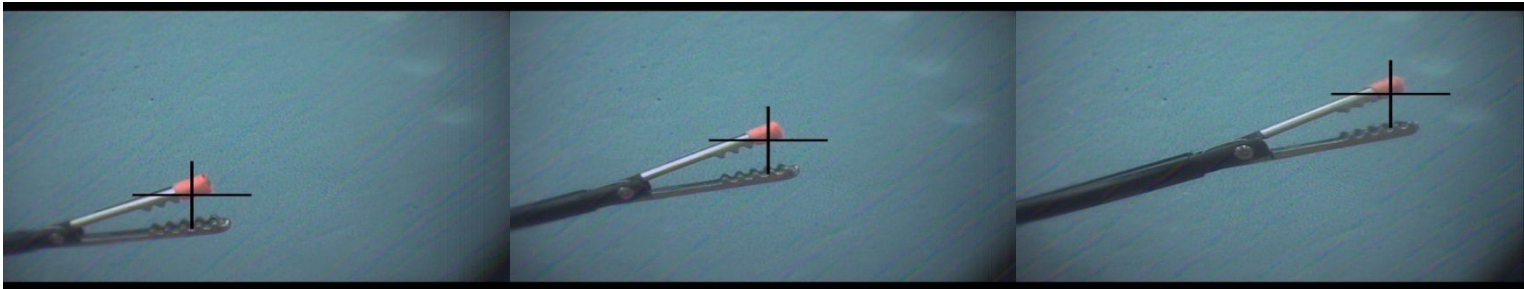


Pan Motor Bearing

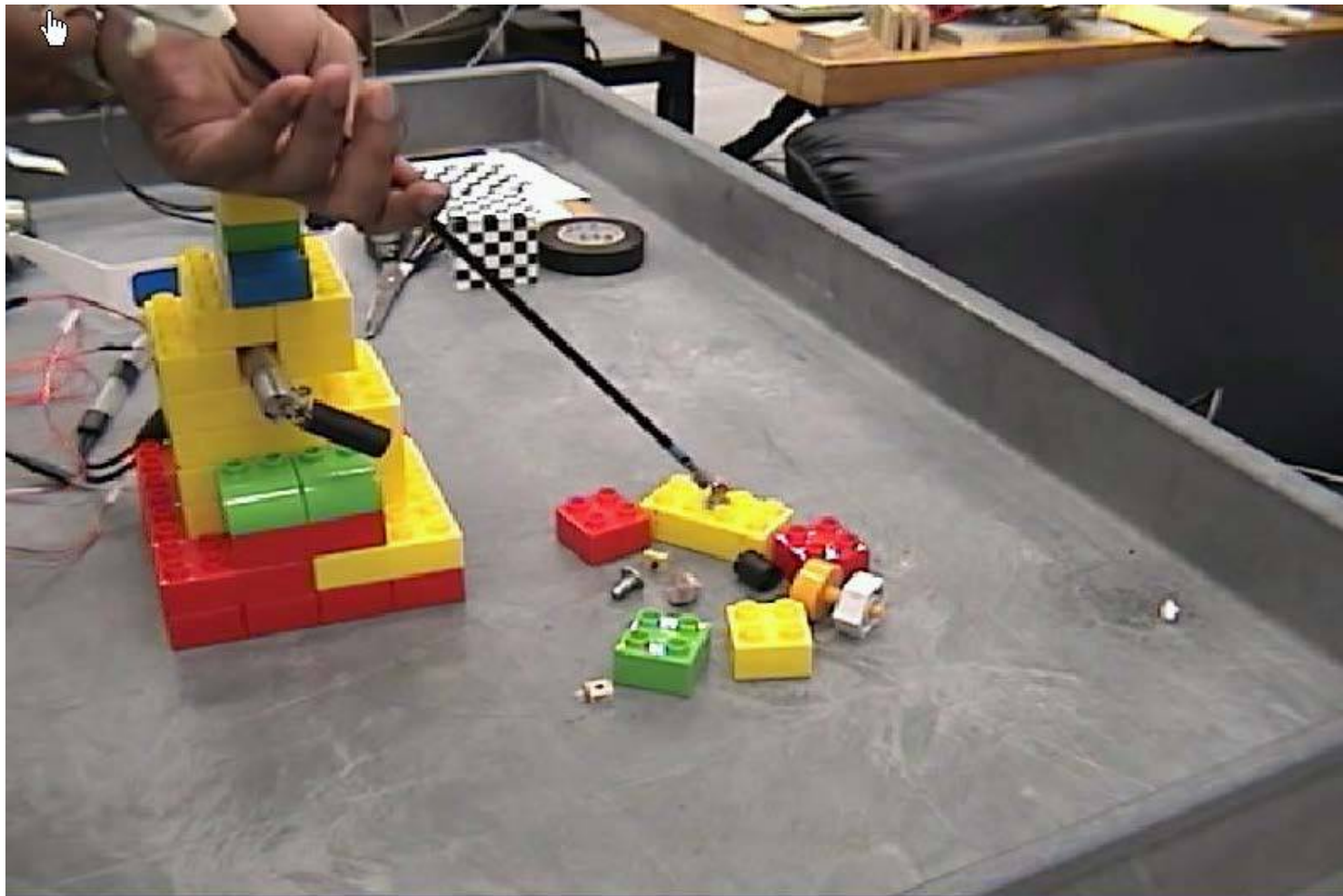
Visual Servoing with Stereo

- When using stereo cameras the pixel disparity E_p between stereo images is used to damp the motors

$$\text{Speed Damping} \propto (\gamma * E_p)$$
- Damping is applied to both Pan and Tilt motors
- Prevents the motors from oscillating when instrument is too close to camera

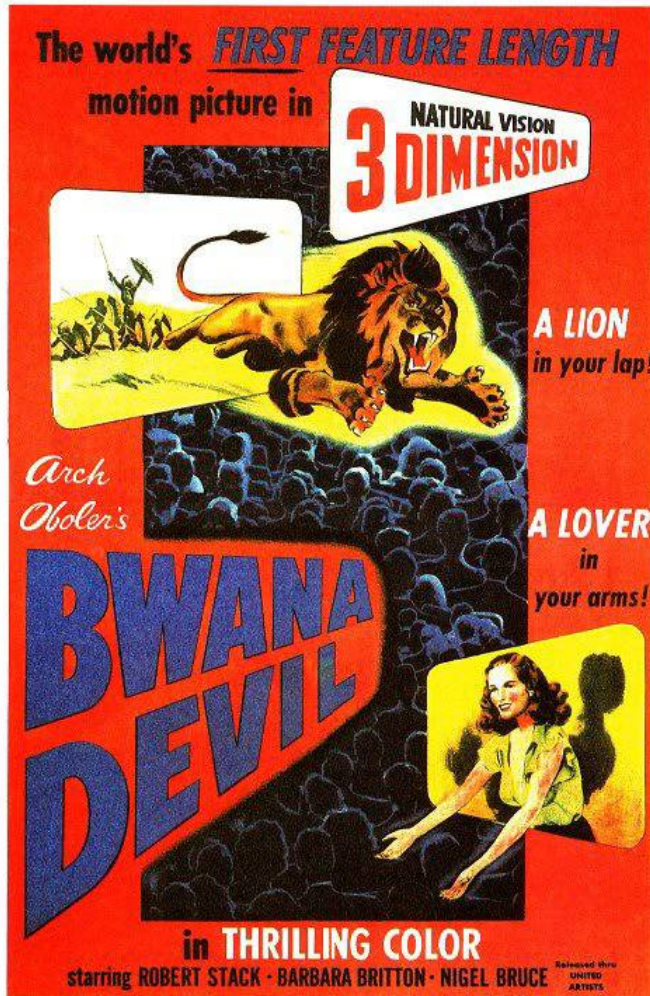


Device III: Stereo Imaging





Caution: 3D viewing ahead !



[Video 1](#)

[Video 2](#)

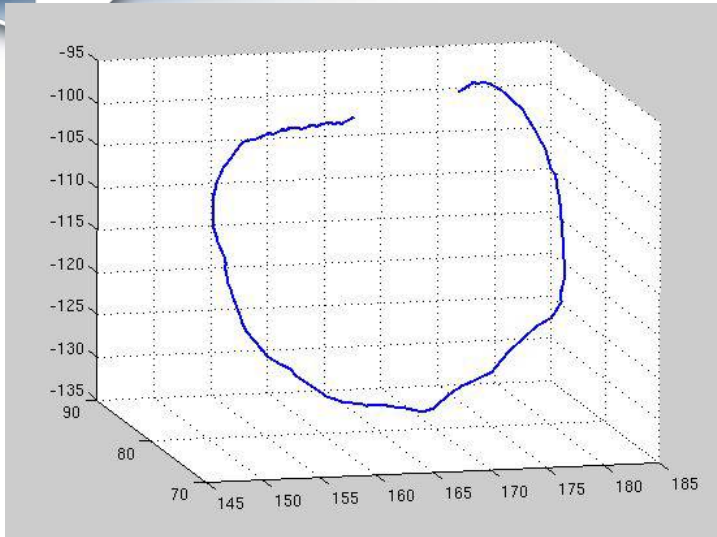




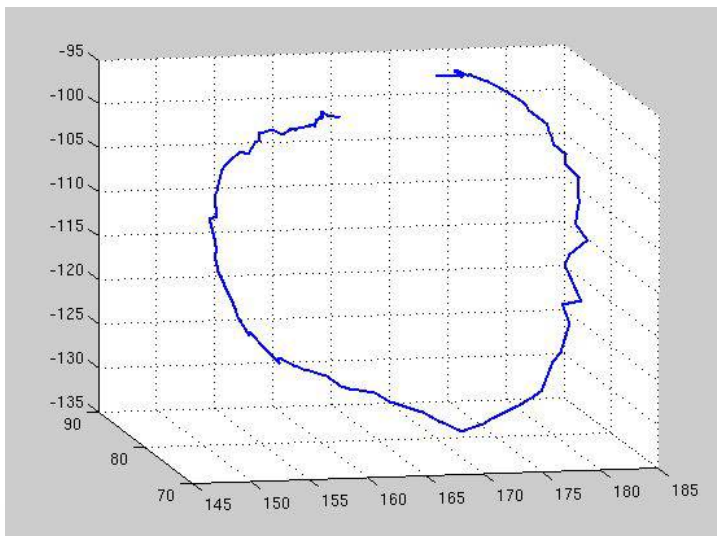
Device III (Stereo) Timings

Procedure	Device	Time (min)
Running Bowel	Laparoscope	5:35
Running Bowel	Robot	3:14
Appendectomy	Laparoscope	1:57
Appendectomy	Robot	1:38
Suturing	Laparoscope	4:30
Suturing	Robot	2:12
Nephrectomy	Robot	9:59

Trajectory Reconstruction



FoB Sensed Trajectory



Stereo Reconstruction of Trajectory

- We traced a trajectory in 3D space using the FoB sensor
- At the same time the sensor was being tracked by our stereo cameras
- The tracking results were used to predict the 3D position of the sensor
- Using this data we plotted the trajectory of the sensor
- average reprojection error ~3mm

Insertable Robotic Effector Platform

The IREP Robot



**K. Xu, R. Goldman, J. Ding, P. Allen, D. Fowler and N. Simaan,
System Design of an Insertable Robotic Effector Platform for Single
Port Access (SPA) Surgery, IROS 2009**



Vision for In-Vivo Surgical Platforms

- IREP Platform integrates vision and tooling: Cameras, Graspers, Dissectors, Scissors, Energy sources
- **Vision** needed for:
 - ◆ Instrument tracking
 - ◆ Kinematic control
 - ◆ 3D measurement/reconstruction
- Vision system is key part of HCI
- Surgeon is focused on the **task**, not controlling the camera images





In-Vivo Tool Tracking*

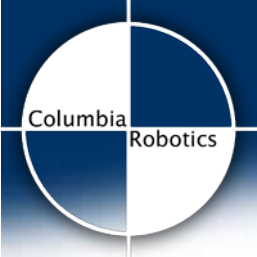
- Tracking in in-vivo surgical environments:
 - ◆ Very dynamic environment
 - ◆ Rapid/Erratic movements
 - ◆ Significant pose changes
 - ◆ Deformable surfaces
 - ◆ Inconsistent lighting, liquid occlusion
 - ◆ Small 3D movements = large 2D non-linear pixel displacements
 - ◆ Frequent broken tracks, lost targets
- What features are best for tracking?
 - ◆ Color? Texture? Geometry?
- Markers or markerless?

*Austin Reiter and Peter Allen, *An Online Approach To In-Vivo Tracking Using Synergistic Features*, IROS 2010



Previous Work: Tool Tracking

- Wei, Arbter, Hirzinger 1997; Groeger, Arbter, Hirzinger 2008 (German Aerospace) – *Custom Color Markers*
- Doignon, Nageotte, de Mathelin 2004; Doignon, Graebbling, de Mathelin 2005; Doignon, Nageotte, de Mathelin 2006 (Univ of Strasbourg) – *Use color without markers*
- Krupa, et. al. 2003 – *Laser Pointing Assistive Device*
- Voros, Long, Cinquin 2007 – *Prior geometry for confinement*
- Pezzementi, Voros, Hager 2009 – *Offline learning of multiple features*
- Mountney, Yang 2008 – *Online feature adaptation for tissue tracking*



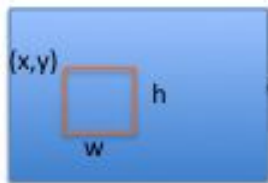
Our Method: Feature Flow

- It's **essential** to *learn new features online*
- Over time, features change as tool moves, lighting changes, occlusions occur – feature set has to evolve and adapt
- Need to automatically discover new parts of your object to track as it moves and turns
- Key Ideas:
 - ◆ Single feature is not enough for robust tracking in-vivo
 - ◆ Synergy: Features working together are better than features working alone
 - ◆ Learning features online is important, when lacking any prior information - even more than offline training
 - ◆ Use likelihood/probability maps to define most promising regions for matching

First Frame

Next Frame

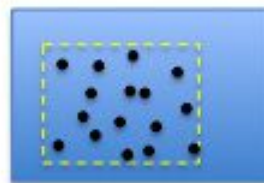
INITIALIZATION



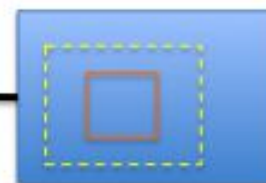
Manual User Nomination^(A)



Extract FAST Corners^(B)

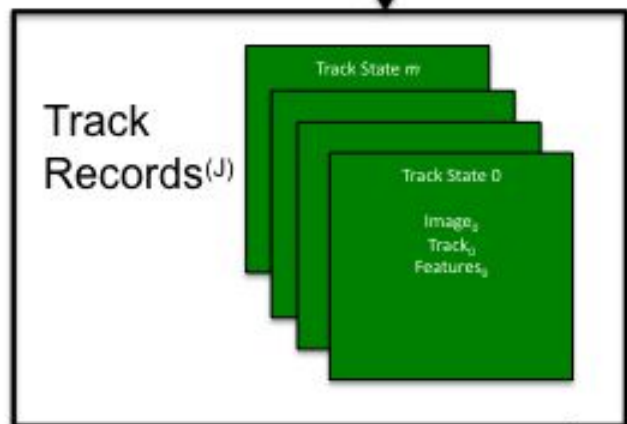


Extract FAST Corners in Expanded Search Region^(D)



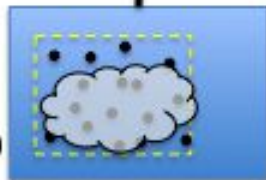
Expand Search Region^(C)

Add 1st State



Add New State

Refine Object Features^(H)



Binary "Object Mask"



Discover new regions

Color Features
Correlation Surface
Gaussian Prior



Construct Likelihood^(F)

Region Growing^(G)

Match Best Track State

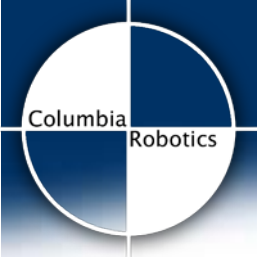
(E)
Track State Alignment Stage

Object Features used as "Seed Points"



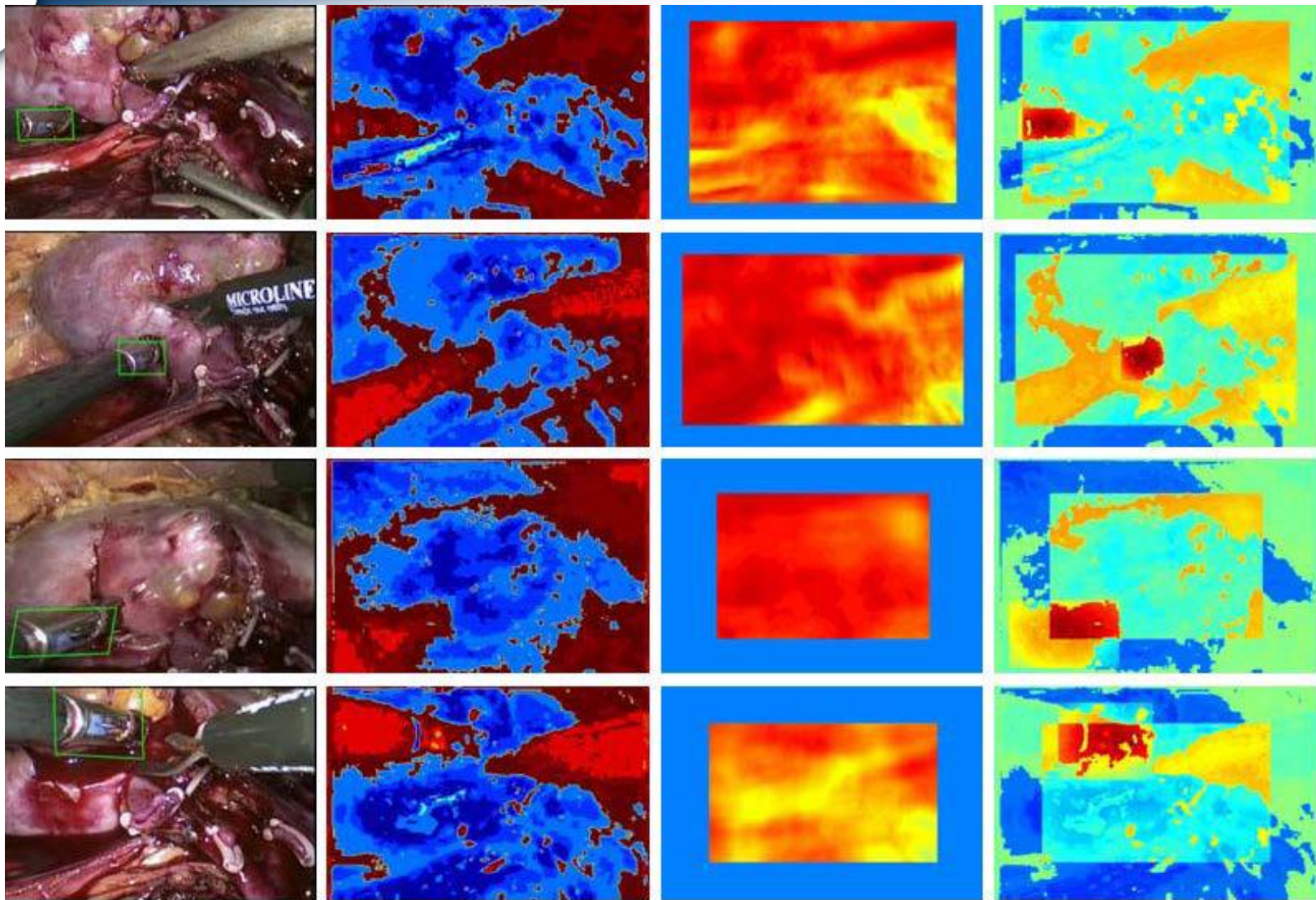
Algorithm

- Initial manual nomination (x,y,width,height)
 - ◆ Extract corners and add first entry to database
- On each successive frame:
 - ◆ Expand search region from previous location (don't want to process entire frame)
 - ◆ Extract corners
 - ◆ Feature matching – normalized cross correlation (NCC) of feature patches
 - ◆ Feature alignment via M-SAC (like RANSAC, but better) – affine model
 - ◆ Evaluate alignment quality – warp proposed track state to current frame and correlate to get similarity measure
 - ◆ Choose *best matching* track state based on alignment metric and add to database
- Note that this part is completely parallelizable



Combining Features/Likelihoods

- Combine multiple features into a composite likelihood map
- Defines which pixels are likely to be our object
- Use a weighted sum of individual probability maps
- We tested three features:
 - ◆ A Gaussian prior, representing where the object alignment estimates the object to be. This will bias us to correct general location.
 - ◆ Normalized Cross Correlation(NCC) surface using a **warped** track frame. Addresses severe pose and deformation changes
 - ◆ Color features: linear combinations of RGB color space, learned from the current environment (Collins et. al. 2005)
- Other features possibility: Region Covariance, Histogram of Oriented Gradients (HOG) or SIFT



Track Frame

Color feature

Correlation

Combined



Feature Flow Results: In-Vivo



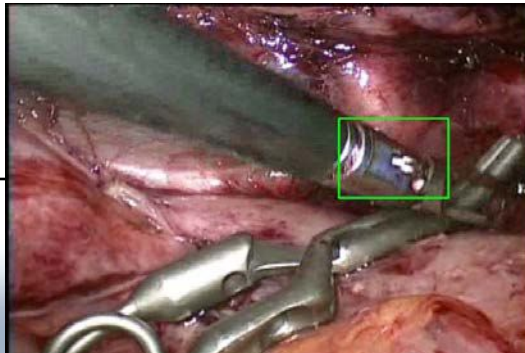
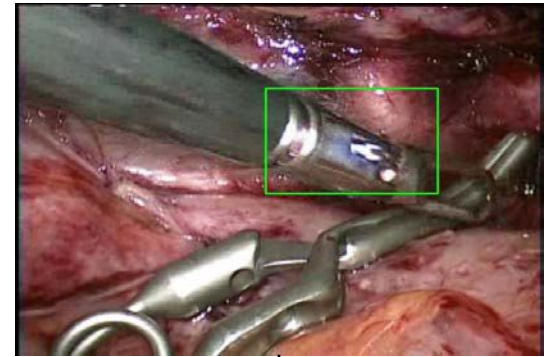
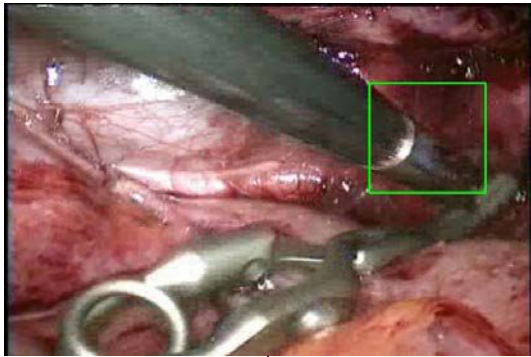
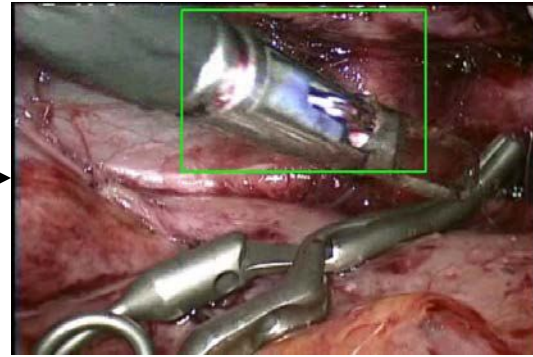
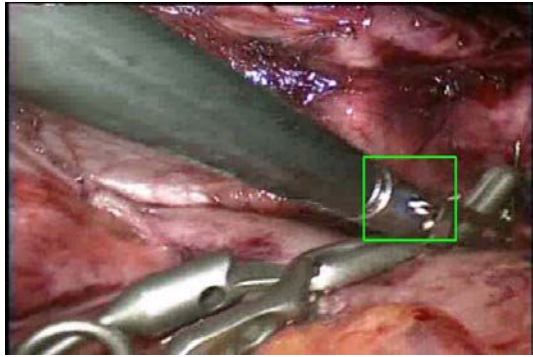


Improvements with Different Feature sets

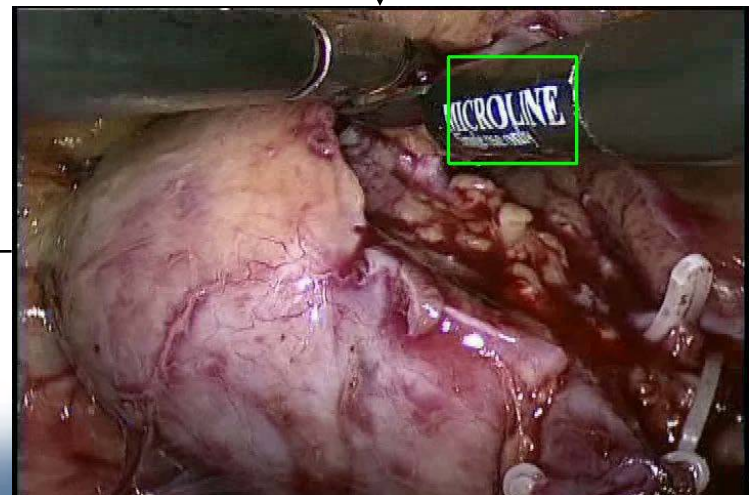
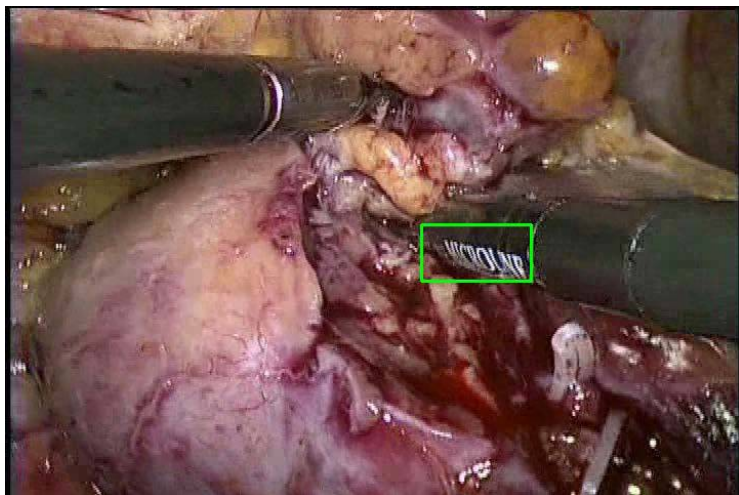
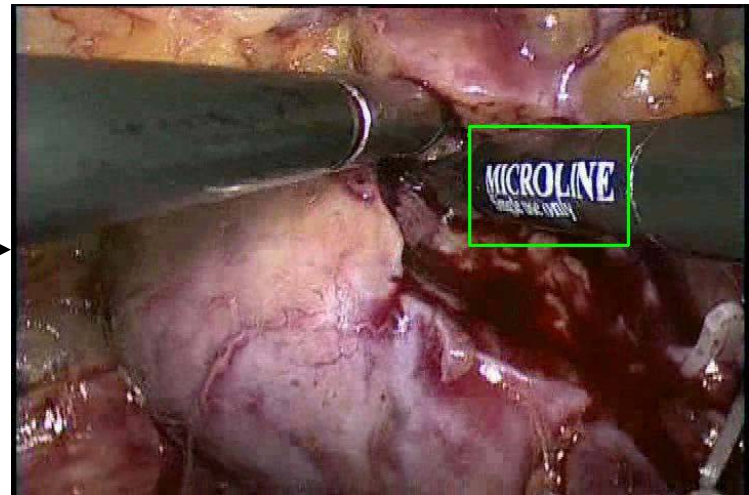
<u>Features</u>	<u>Track Time</u>
No Likelihood Discovery	1:01
NCC (No Warp)	1:16
Color (Alone)	1:44
NCC (With Warp)	1:55
Color and NCC (With Warp)	2:17

Real-time performance: 12fps

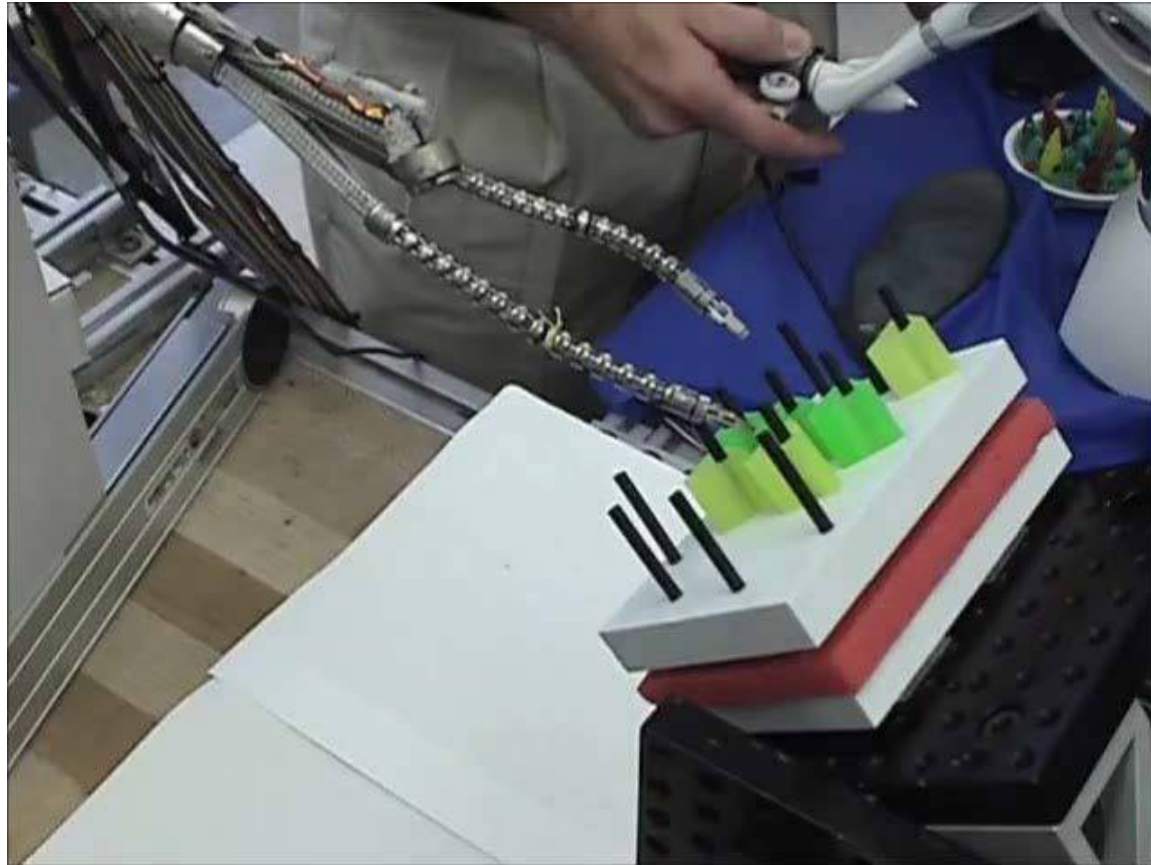
Size and Pose Changes



A Different Tool – Text Label



Continuum Robot Pose Estimation

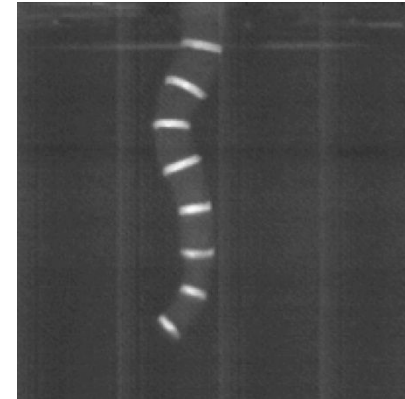


A Learning Algorithm for Visual Pose Estimation of Continuum Robots,
A. Reiter, R. Goldman, A. Bajo, K. Iliopoulos, N. Simaan, P. Allen, IROS 2011

Previous Work

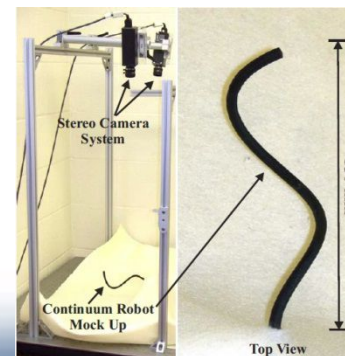
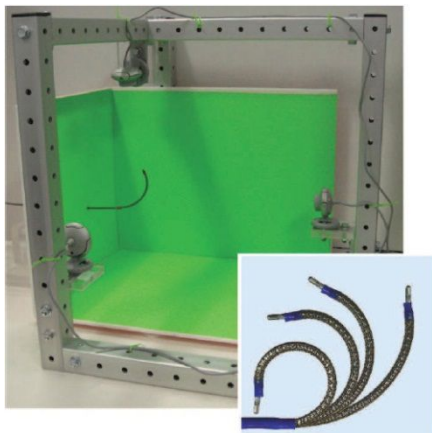
Hannan & Walker (2003)

- Extract vertebrae
- Fit successive circles
- Curvature comes from change in segment length due to bending



Camarillo, et. al. (2008)

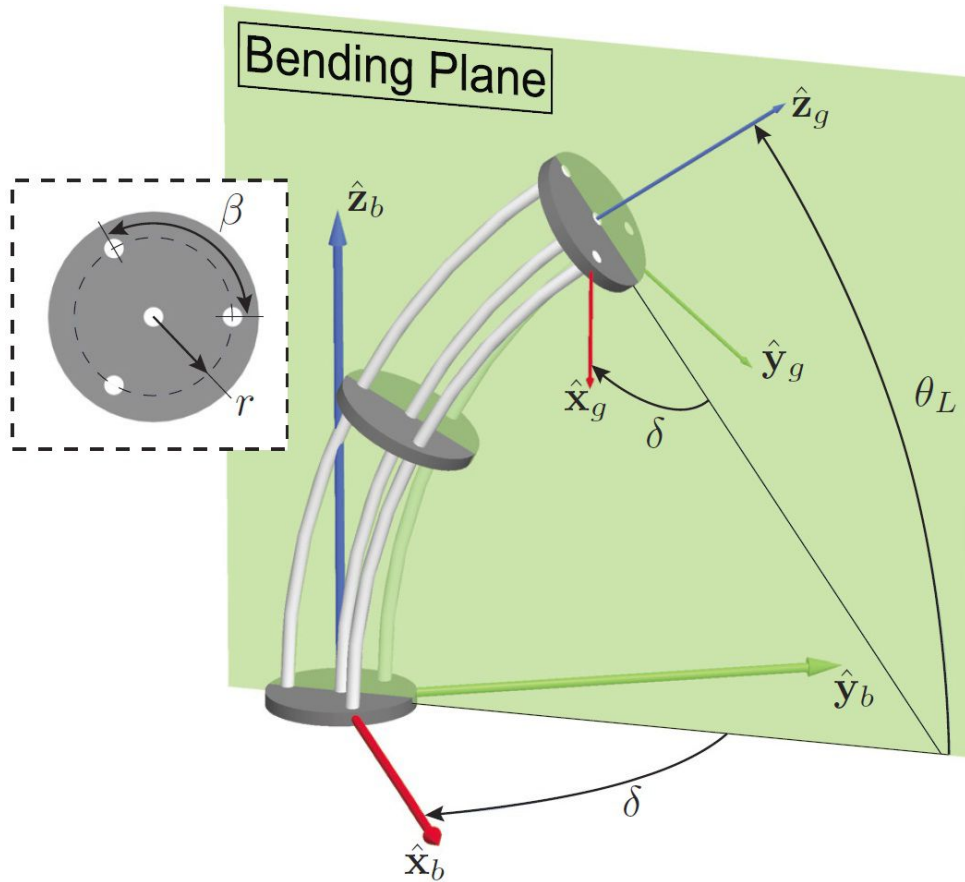
- Voxel carving
- 3 orthogonal cameras
- High positional precision of flexible manipulator



Croom, et. al. (2010)

- Stereo SOMs
- No fiducials
- Detected shape of continuum robot

Continuum Segment Model



$$\psi = [\theta_L, \delta]^T$$



$$\theta_L = \theta_0 - \text{atan2} \left(\sqrt{R_{13}^2 + R_{23}^2}, R_{33} \right)$$

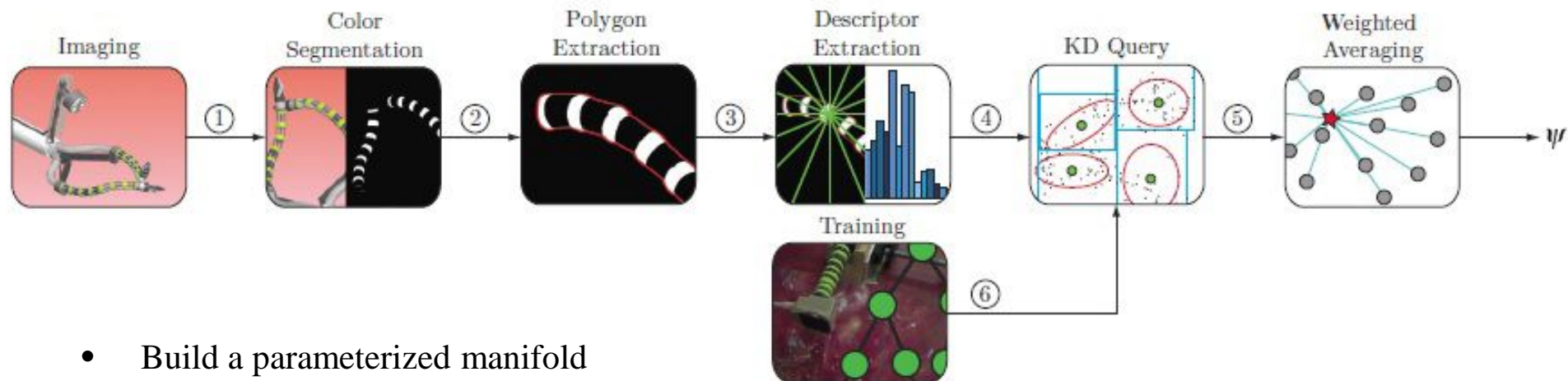
$$\delta = -\text{atan2} (R_{23}, R_{13})$$

$\theta_0 = \pi/2$

$$\mathbf{R} = \mathbf{R}_z \mathbf{R}_y \mathbf{R}_z^T$$

Orientation of the end disk

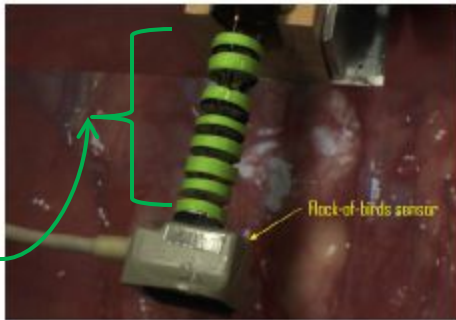
Visual Learning Overview



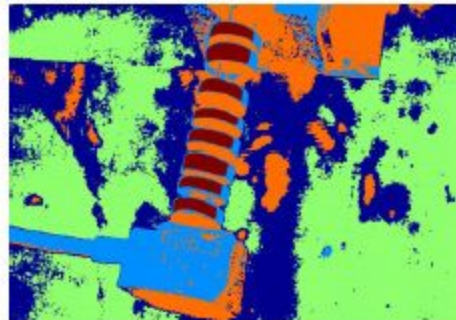
- Build a parameterized manifold using (compressed) feature descriptors
- Manifold is parameterized by robot DOFs
- Unknown configurations looked-up using weighted average of nearest neighbors in manifold

Image Segmentation

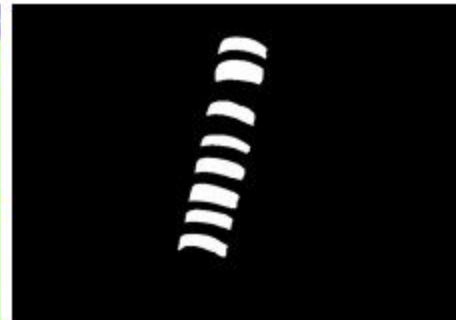
Concave Polygon



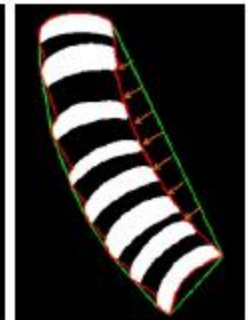
(a) Color Image



(b) Cluster Labels



(c) Segmented Image



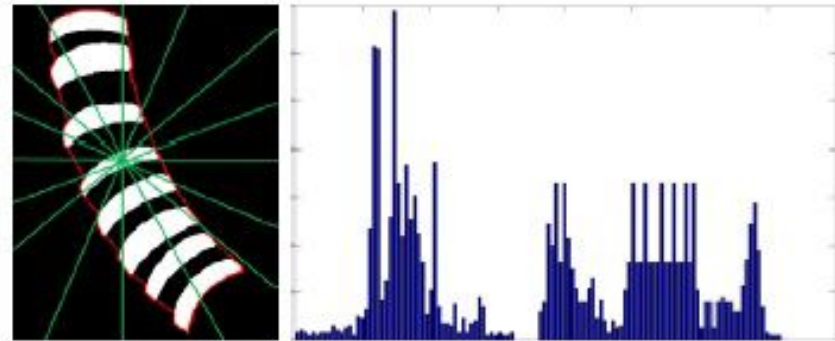
(d) Contour

Lime Green Fiducials (want to *stick out* in surgical imagery)

K-Means Clustering in CIELAB-color space

Feature Descriptor

- Locate center of binary mask using median of marked pixels
- Compute angle of each point along red contour w.r.t. center
- Fill histogram
 - Experimented with different bin sizes: 72 (5°), **120 (3°)**, and 360 (1°)
- Extract separately from stereo images and combine as composite feature vector

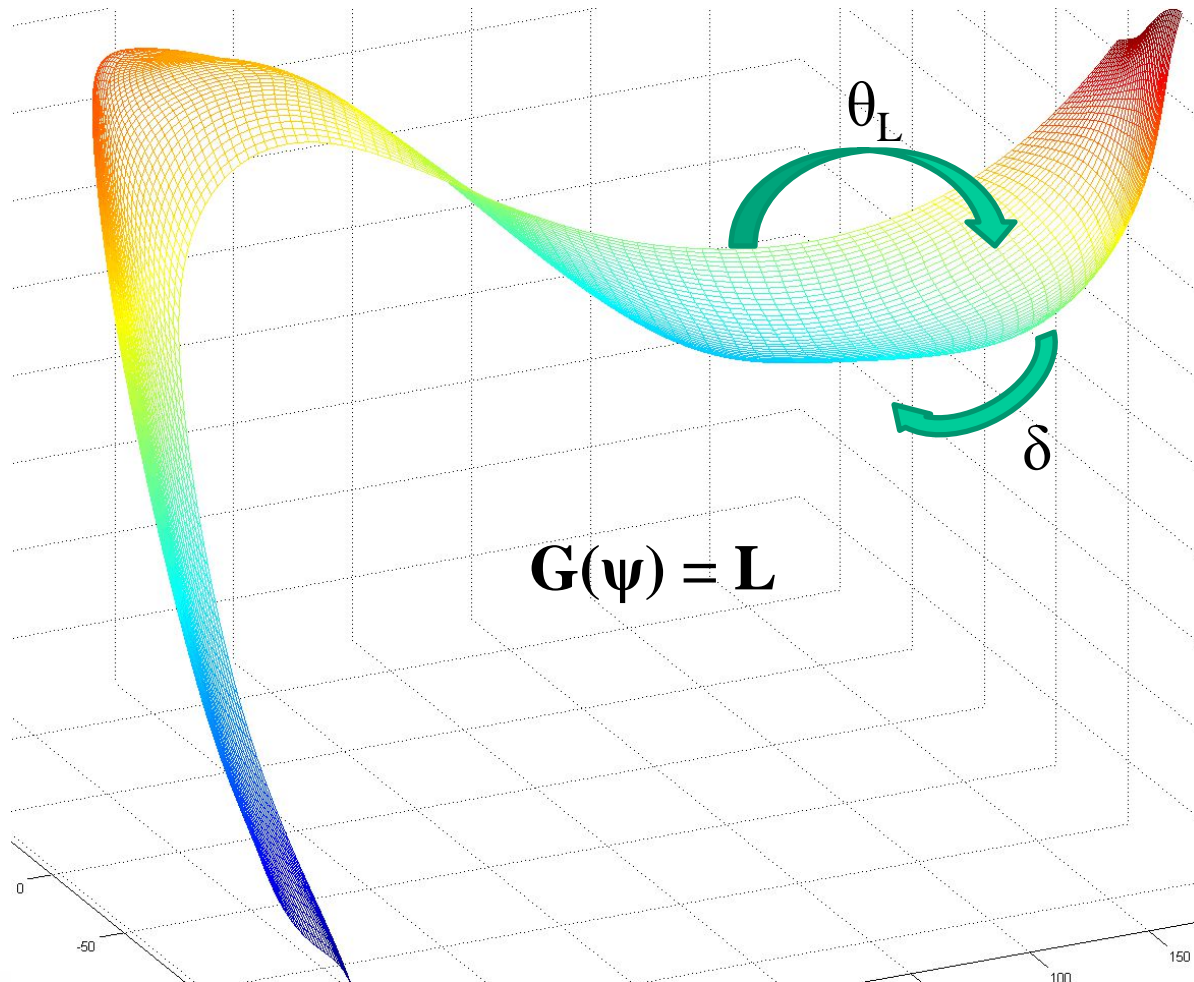




Training Data

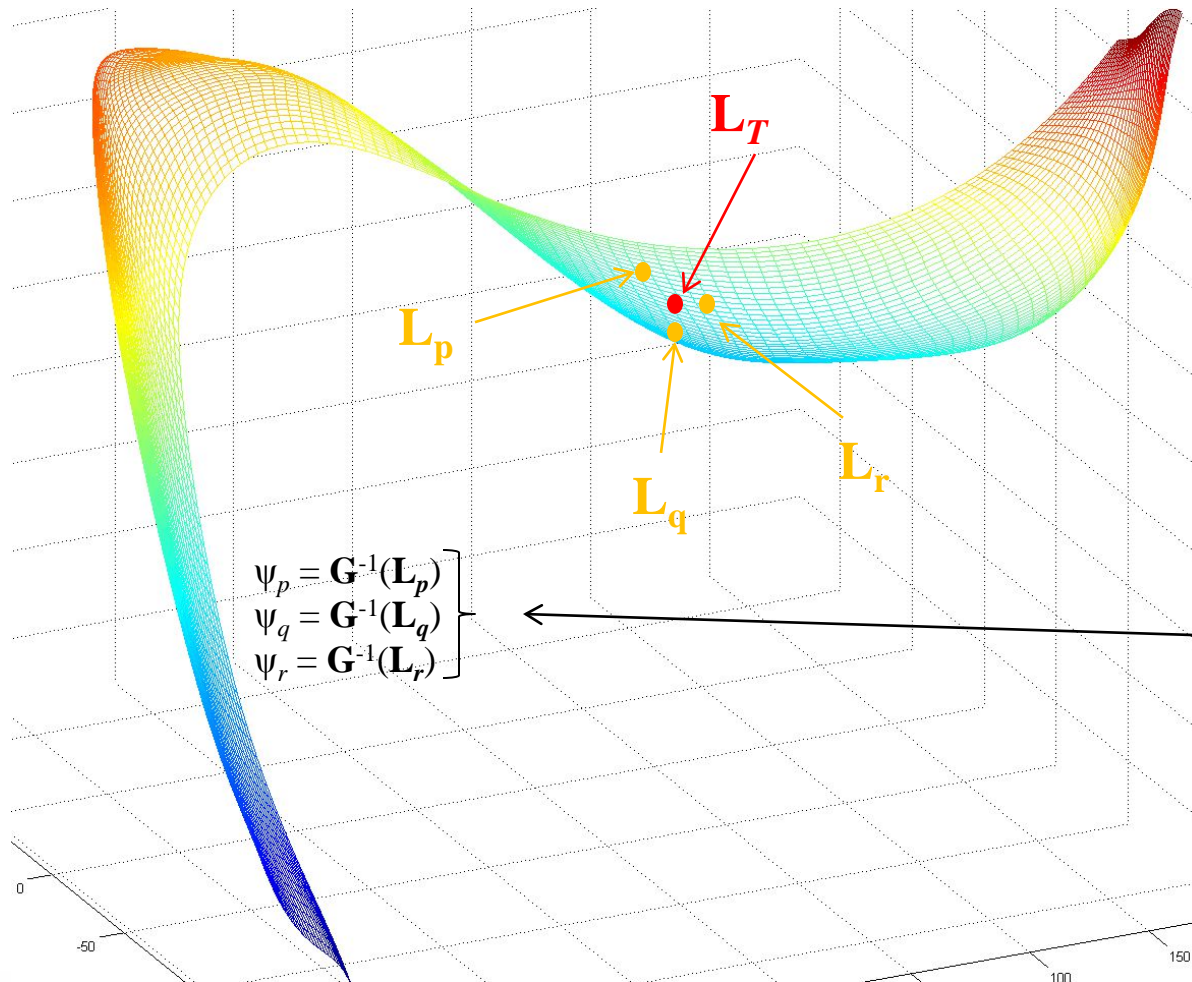
- Pre-processing
 - ◆ Reduce high-dimensional stereo composite feature using PCA, called *eigen-features*
 - ◆ Experiment with different variance recoveries (65%, 85%, **90%**, 95%) with different bin sizes
- Interpolate smooth manifold (spline) using compressed vectors
 - ◆ Parameterize on ψ -angles (2 DOFs), which yields a surface
 - More DOFs would lead to a volume, etc...

Descriptor Manifold



- Surface of *eigen-features* (2 DOFs)
- 2x120-bins reduced to 16 dimensions
- Only first 3 dimensions of eigen-projections shown, for convenience

Configuration Query

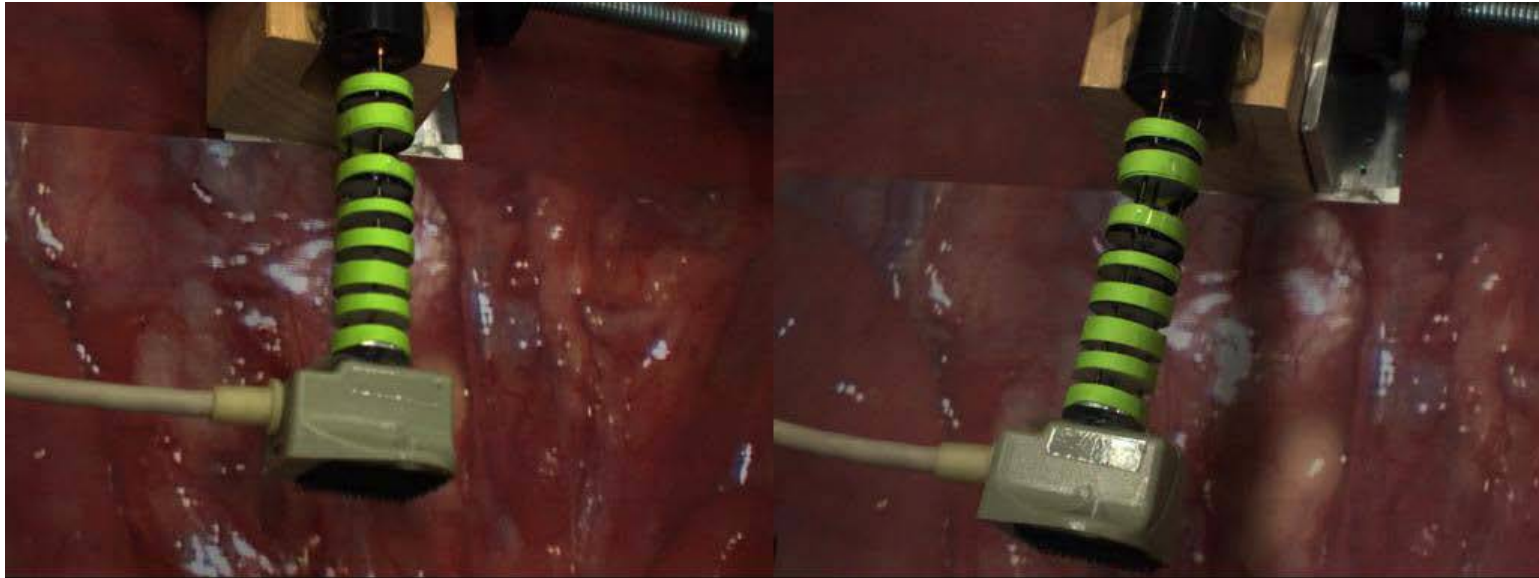


\mathbf{L}_T : query descriptor
(unknown configuration)

$\mathbf{L}_p, \mathbf{L}_q, \mathbf{L}_r$: nearest-
neighbor matches from
manifold (created by
training data)

- Recover configuration parameters which created those interpolated values
- Weighted average of nearest neighbors based on distance on manifold

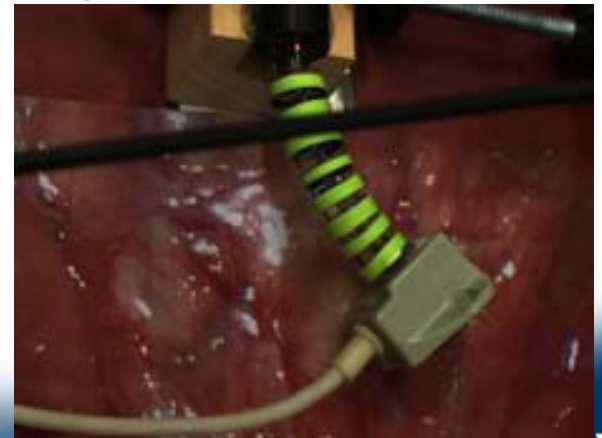
Experimental Setup



- Stereo camera system made up of 2 Point Grey Dragonfly2 cameras (1024x768, color)
- Manually-actuated single-segment snake arm
 - ◆ Lime green markers for segmentation
 - ◆ Flock-of-Birds at tip for pose ground truth
 - ◆ Background of printouts from laparoscopic procedure for more realistic setting

Accuracy

- Different combinations of histogram bin-size and variance recovery
 - ◆ 360, 120, and 72-bins (each x2)
 - ◆ 65%, 85%, 90%, 95%
 - ◆ Best tradeoff performance from 120-bin histograms (stereo feature $\in \mathbb{R}^{240}$) reduced to 90% variance $\in \mathbb{R}^{16}$
- Exp. 1: no occlusions, testing data **not** included in training data
 - ◆ ~ 800 frames
 - ◆ $[\varepsilon_\delta = 0.98^\circ, \varepsilon_{\theta_L} = 1.28^\circ]$, 1.16° median error
- Exp. 2: occlusion from laparoscopic tool, testing data **not** included in training data
 - ◆ ~ 600 frames
 - ◆ $[\varepsilon_\delta = 1.04^\circ, \varepsilon_{\theta_L} = 2.06^\circ]$, 1.46° median error





Summary

Columbia In-vivo Camera:

- Easier and more intuitive to use than a standard laparoscope.
- Insertion port available for tooling
- Joystick operation requires no specialized operator training.
- Pan/Tilt functions provide large imaging volume
- Time to perform procedures was better or equivalent
- Automatic Tracking and Visual Servoing assist surgeon
- 3D vision improves the visualization and depth perception
- Cost effective, perhaps single-use or modular replacement

IREP Robot:

- Integrated platform for imaging and effectors
- Vision system can be used to close the control loop of effectors

Markerless Tool Tracking:

- Long term tracking with recovery
- Adaptive online feature learning
- Real-time performance

Pose Estimation:

- Learning-based method is accurate for recovering pose



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- Austin Reiter
- Dennis Fowler
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